Filtering in the Fourier Domain

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Fourier Filtering

- Low-pass filtering
- High-pass filtering
- Band-pass filtering
- Sampling and aliasing
- Tomography
- Optimal filtering and match filters

Some Identities to Remember

Fourier Spectrum–Rotation

Phase vs Spectrum

Image Reconstruction from phase map

Reconstruction from spectrum

Low-Pass Filter

- Reduce/eliminate high frequencies
- Applications
	- Noise reduction
		- uncorrelated noise is broad band
		- Images have sprectrum that focus on low frequencies

Ideal LP Filter – Box, Rect

Extending Filters to 2D (or higher)

- Two options
	- Separable
		- \cdot H(s) -> H(u)H(v)
		- Easy, analysis
	- Rotate
		- H(s) -> H((v² + v²)^{1/2})
		- Rotationally invariant

Ideal LP Filter – Box, Rect

Ideal Low-Pass Rectangle With Cutoff of 2/3

Ideal LP – 1/3

Ideal LP – 2/3

Butterworth Filter

Lowpass filters. D_0 is the cutoff frequency and *n* is the order of the Butterworth filter.

Butterworth - 1/3

Butterworth vs Ideal LP

Butterworth – 2/3

Gaussian LP Filtering

ILPF BLPF GLPF

F1

F2

High Pass Filtering

- HP = 1 LP
	- All the same filters as HP apply
- Applications
	- Visualization of high-freq data (accentuate)
- High boost filtering

 $-$ HB = (1 - a) + a(1 - LP) = 1 - a*LP

High-Pass Filters

FIGURE 4.52 Top row: Perspective plot, image representation, and cross section of a typical ideal highpass filter. Middle and bottom rows: The same sequence for typical Butterworth and Gaussian highpass filters.

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High-Pass Filters in Spatial Domain

a b c

FIGURE 4.53 Spatial representation of typical (a) ideal, (b) Butterworth, and (c) Gaussian frequency domain highpass filters, and corresponding intensity profiles through their centers.

High-Pass Filtering with IHPF

FIGURE 4.54 Results of highpass filtering the image in Fig. 4.41(a) using an IHPF with $D_0 = 30$, 60, and 160.

a b c

FIGURE 4.55 Results of highpass filtering the image in Fig. 4.41(a) using a BHPF of order 2 with $D_0 = 30, 60$, and 160, corresponding to the circles in Fig. 4.41(b). These results are much smoother than those obtained with an IHPF.

GHPF

a b c

FIGURE 4.56 Results of highpass filtering the image in Fig. 4.41(a) using a GHPF with $D_0 = 30$, 60, and 160, corresponding to the circles in Fig. 4.41(b). Compare with Figs. 4.54 and 4.55.

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High Boost with GLPF

High-Boost Filtering

Band-Pass Filters

• Shift LP filter in Fourier domain by convolution with delta

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Band Pass - Two Dimensions

- Two strategies
	- Rotate
		- Radially symmetric
	- Translate in 2D
		- Oriented filters

- Note:
	- Convolution with delta-pair in FD is multiplication with cosine in spatial domain

Band Bass Filtering

Radial Band Pass/Reject

Band Reject Filtering

Band Reject Filtering

Band Reject Filtering

Discrete Sampling and Aliasing

- Digital signals and images are discrete representations of the real world
	- Which is continuous
- What happens to signals/images when we sample them?
	- Can we quantify the effects?
	- Can we understand the artifacts and can we limit them?
	- Can we reconstruct the original image from the discrete data?

A Mathematical Model of Discrete Samples

Delta functional

A Mathematical Model of Discrete Samples

• Goal

– To be able to do a continuous Fourier transform on a signal before and after sampling

Discrete signal

 f_k $k = 0, \pm 1, ...$

Samples from continuous function

 $f_k = f(k\Delta T)$

Representation as a function of t • Multiplication of f(t) with Shah $\tilde{f}(t) = f(t) s_{\Delta T}(t) = \sum_{k=0}^{\infty} f_k \delta(t - k \Delta T)$ $k=-\infty$

Fourier Series of A Shah Functional

Fourier Transform of A Discrete Sampling

$$
\tilde{f}(t) = f(t)s(t)
$$
 \longleftrightarrow $\tilde{F}(u) = F(u) * S(u)$

Fourier Transform of A Discrete Sampling

What if F(u) is Narrower in the Fourier Domain?

- No aliasing!
- How could we recover the original signal?

What Comes Out of This Model

- Sampling criterion for complete recovery
- An understanding of the effects of sampling
	- Aliasing and how to avoid it
- Reconstruction of signals from discrete samples

Shannon Sampling Theorem

• Assuming a signal that is band limited:

 $f(t) \longrightarrow F(u)$ $|F(u)| = 0 \forall |u| > B$

- Given set of samples from that signal $\Delta T \leq \frac{1}{2B}$ $f_k = f(k \Delta T)$
- Samples can be used to generate the original signal
	- Samples and continuous signal are equivalent

Sampling Theorem

- Quantifies the amount of information in a signal
	- Discrete signal contains limited frequencies
	- Band-limited signals contain no more information then their discrete equivalents
- Reconstruction by cutting away the repeated signals in the Fourier domain
	- Convolution with sinc function in space/time

Reconstruction

• Convolution with sinc function

 $f(t) = \tilde{f}(t) * \mathbb{F}^{-1} \left[\text{rect}\left(\frac{\mathbf{u}}{\Delta T}\right) \right]$ $= \left(\sum_k f_k \delta(t - k\Delta T)\right) * \operatorname{sinc}\left(\frac{t}{\Delta T}\right) = \sum_k f_k \operatorname{sinc}\left(\frac{t - k\Delta T}{\Delta T}\right)$ $-1\frac{1}{0}$ 5 \mathbf{a} $\mathbf{1}$

Sinc Interpolation Issues

- Must functions are not band limited
- Forcing functions to be band-limited can cause artifacts (ringing)

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Ringing - Gibbs phenomenon Other issues:

Sinc is infinite - must be truncated

Aliasing

• High frequencies appear as low frequencies when undersampled

Aliasing

Overcoming Aliasing

- Filter data prior to sampling
	- Ideally band limit the data (conv with sinc function)
	- In practice limit effects with fuzzy/soft low pass

Antialiasing in Graphics

• Screen resolution produces aliasing on underlying geometry

Antialiasing

Interpolation as Convolution

• Any discrete set of samples can be considered as a functional

$$
\tilde{f}(t) = \sum_{k} f_k \delta(t - k \Delta T)
$$

- Any linear interpolant can be considered as a convolution
	- Nearest neighbor rect(t)

\n**Linear - trift**\n

\n\n
$$
\text{tri}(t) =\n \begin{cases}\n t + 1 & -1 \leq t \leq 0 \\
1 - t & 0 \leq t \leq t \\
0 & \text{otherwise}\n \end{cases}
$$
\n

Convolution-Based Interpolation

- Can be studied in terms of Fourier Domain
- Issues
	- Pass energy (=1) in band
	- Low energy out of band
	- Reduce hard cut off (Gibbs, ringing)

Tomography Formulation

Attenuation

$$
I = I_0 \exp\left(-\int \mu(x, y) ds\right)
$$

$$
p(r, \theta) = \ln(I/I_0) = -\int \mu(x, y) ds
$$

Line with angle theta

Log gives line integral

$$
x\cos\theta + y\sin\theta = r
$$

Volume integral

$$
p(r, \theta) =
$$

$$
\int_{-\infty}^{\infty} \int_{-\infty}^{\infty} f(x, y) \delta(x \cos \theta + y \sin \theta - r) dx dy
$$

